

# Contributions of Time-of-Flight cameras for Biomedical Applications

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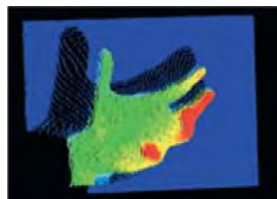
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# Content

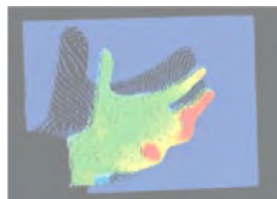
- 1 Introduction/Motivation
- 2 Time-of-Flight (ToF) principle
- 3 Biomedical ToF applications
  - MUSTOF 3-D endoscopy
  - Respiratory motion gating
  - Patient positioning
- 4 Summarize
- 5 Outlook





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# State of the Art

## Time-of-Flight (ToF) technology

- Lateral resolution:  $120 \times 160$  pixel
- Depth resolution: 3 mm
- Wavelength: 870 nm
- Pixel dimension:  $40 \mu m \times 40 \mu m$
- Modulation frequency: 20 MHz ( $\Rightarrow \lambda = 15m$ )
- Frame rate:  $>12$  fps



Figure: ToF-camera and example images



# State of the Art

## Time-of-Flight (ToF) technology

- Lateral resolution:  $176 \times 144$  pixel
- Depth resolution: 2,5 mm
- Wavelength: 870 nm
- Pixel dimension:  $40\mu m \times 40\mu m$
- Modulation frequency: 20 MHz ( $\Rightarrow \lambda = 15m$ )
- Frame rate: >25 fps

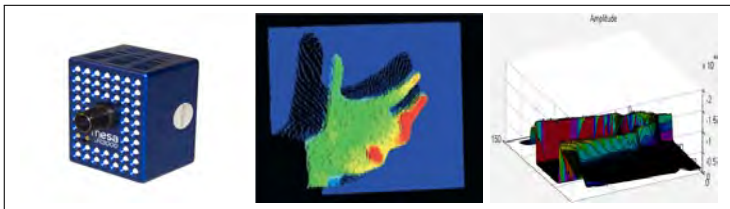
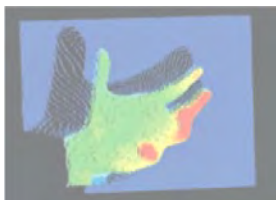


Figure: ToF-camera and example images



# Overview

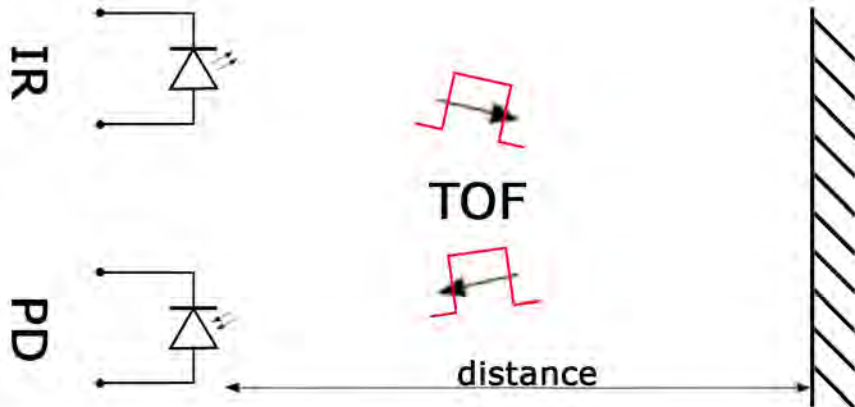
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# Time-of-flight principle

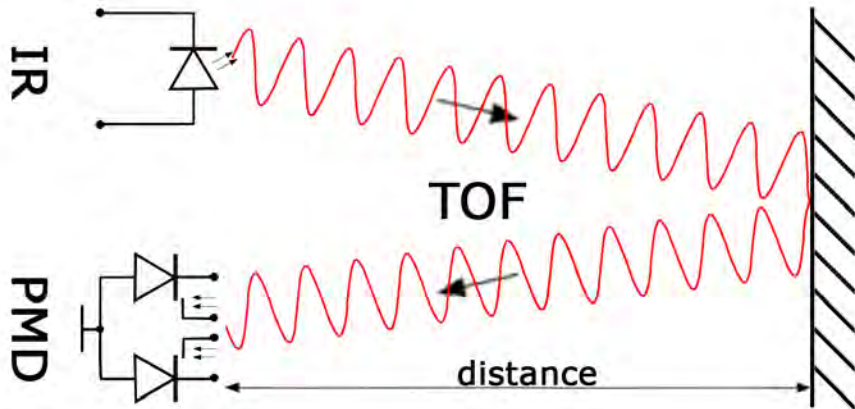
Pulsed modulation





# Time-of-flight principle

## Continuous wave modulation







# Time-of-flight principle

## Continuous wave modulation

- Infra-red light with amplitude modulation using a modulation frequency  $f_{mod}$  is sent out by the camera (active illumination), scattered by the object and received again by the camera after a **time of flight**  $\tau_d$ .
- The camera measures the **phase difference**  $\varphi_d$  between the sent signal  $g_k(t)$  with phasing  $\varphi_T$  and the reflected and received wave  $s_d(t) \sim g_k(t - \tau_d)$  with phasing  $\varphi_R$ .

$$\varphi_d = \varphi_R - \varphi_T = 2\pi f_{mod} \tau_d \quad (1)$$

- Assuming constant speed of light  $c$  the **distance**  $d$  is proportional to the phase shift  $\varphi_d$  of emitted and reflected wave:

$$d = \frac{c \cdot \varphi_d}{4\pi \cdot f_{mod}} \quad [Heinol 2001] \quad (2)$$



# Time-of-flight principle

## Measurement cycles

- The phase difference is measured by **sampling the received signal** at  $N$  equidistant measurement points. This can be realised by a **stepwise increased phase shift**  $\bar{\omega}\tau_k$  of the electrical reference signal:

$$\bar{\omega}\tau_k = \frac{2\pi}{N} \cdot (k - 1) \text{ with } k = 1, 2, \dots, N \text{ [Luan 2001]} \quad (3)$$

For normally applied  $N = 4$  this means an iterative phase shift by  $90^\circ$  with  $\bar{\omega}\tau_1 = 0^\circ$  and  $\bar{\omega}\tau_4 = 270^\circ$



# Time-of-flight principle

## Correlation function

- With the **correlation function**  $c(\tau_k) = s_d(t) \otimes g_k(t + \tau_k)$

$$c(\tau_k) = \frac{a}{2} \cdot \cos(\varphi_d + \bar{\omega}\tau_k) \quad [\text{Lange 2000}] \quad (4)$$

and the **voltage dependency**

$$U_k \sim K + c(\tau_k) \quad (K : \text{background illumination influence}) \quad (5)$$

the resulting voltages  $U_k$  can be computed as

$$\begin{aligned} U_1 &\sim K + \frac{a}{2} \cdot \cos(\varphi_d), & U_2 &\sim K - \frac{a}{2} \cdot \sin(\varphi_d), \\ U_3 &\sim K - \frac{a}{2} \cdot \cos(\varphi_d), & U_4 &\sim K + \frac{a}{2} \cdot \sin(\varphi_d). \end{aligned} \quad (6)$$



# Time-of-flight principle

## Results

- Thus a pair of phase shift depending **voltage differences**  $\Delta U_{31}$  and  $\Delta U_{24}$  can be build:

$$\begin{aligned}\Delta U_{24} &= U_2 - U_4 = -a \cdot \sin(\varphi_d) \\ \Delta U_{31} &= U_3 - U_1 = -a \cdot \cos(\varphi_d)\end{aligned}\quad (7)$$

- The relation of these two voltage differences is depending on  $\varphi$

$$\frac{\Delta U_{24}}{\Delta U_{31}} = \tan(\varphi_d)\quad (8)$$

but without knowledge of the unit circle quadrant the common arcustangens function is not sufficient to compute  $\varphi$  unambiguously for the range of values between 0 and  $2\pi$  .



# Time-of-flight principle

## Results

- Using the two-argument function `atan2` to handle the ambiguity and shifting the results from a range of  $-\pi \dots \pi$  back to  $0 \dots 2\pi$  one finally can compute the **phase shift**  $\varphi_d$ :

$$\varphi_d = \text{atan2}(\Delta U_{24}, \Delta U_{31}) + \pi \quad (9)$$

- Amplitude**  $A$  depends as well on  $\Delta U_{24}$  and  $\Delta U_{31}$

$$A \sim \frac{\sqrt{\Delta U_{24}^2 + \Delta U_{31}^2}}{2} \quad (10)$$

- Offset**  $K$  can be computed with voltages  $U_1 \dots U_4$

$$K \sim \frac{U_1 + U_2 + U_3 + U_4}{4} \quad (11)$$



# ToF accuracy

## Illumination requirements

- small light emitting surface
- high power
- fast modulation
- narrow-band for ambient light suppression

$$\text{accuracy} = \frac{c}{2f_{mod}} \cdot \sqrt{\frac{P_{mod} + P_{amb}}{P_{mod}^2} \frac{A}{k_{opt}q_e r T}}$$

$c$  : relative speed of light  
 $f_{mod}$  : modulation frequency  
 $P_{laser}$  : power of modulated signal  
 $P_{amb}$  : ambient light power  
 $A$  : illuminated area

$k_{opt}$  : optical system constant  
 $q_e$  : quantum efficiency  
 $r$  : target reflectivity  
 $T$  : integration time



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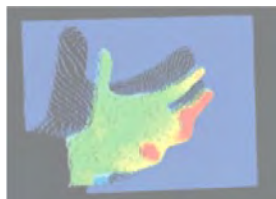
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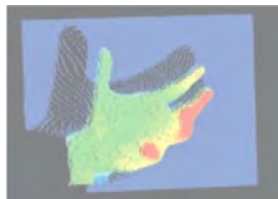
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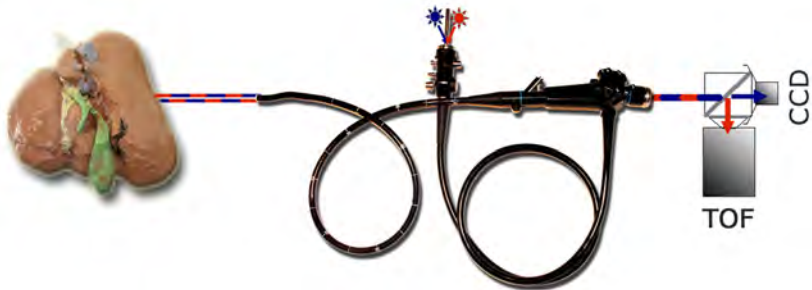


# Idea of MUSTOF

Parallel acquisition with ToF camera and CCD camera

Parallel acquisition of depth and image data combining a ToF and a CCD chip:

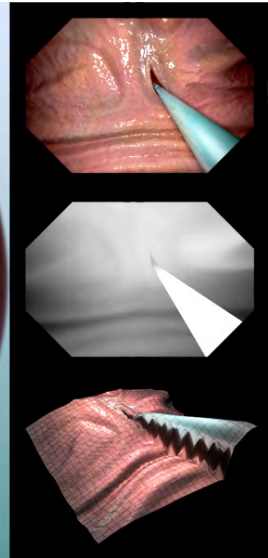
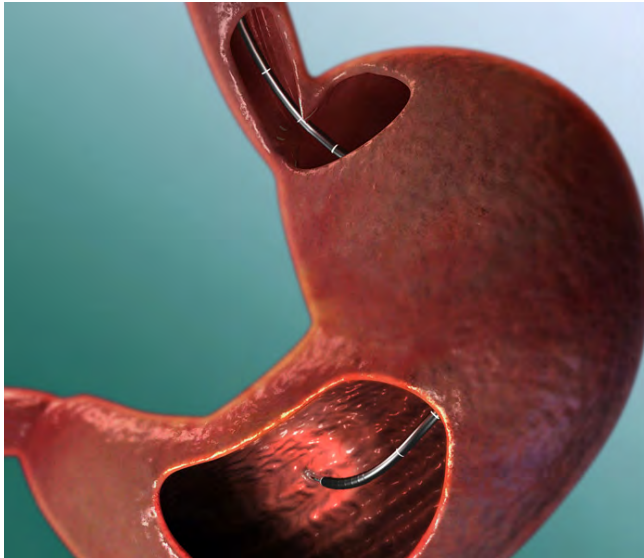
MultiSensorTimeOfFlight (MUSTOF) endoscope





# Navigation support - Off-axis view

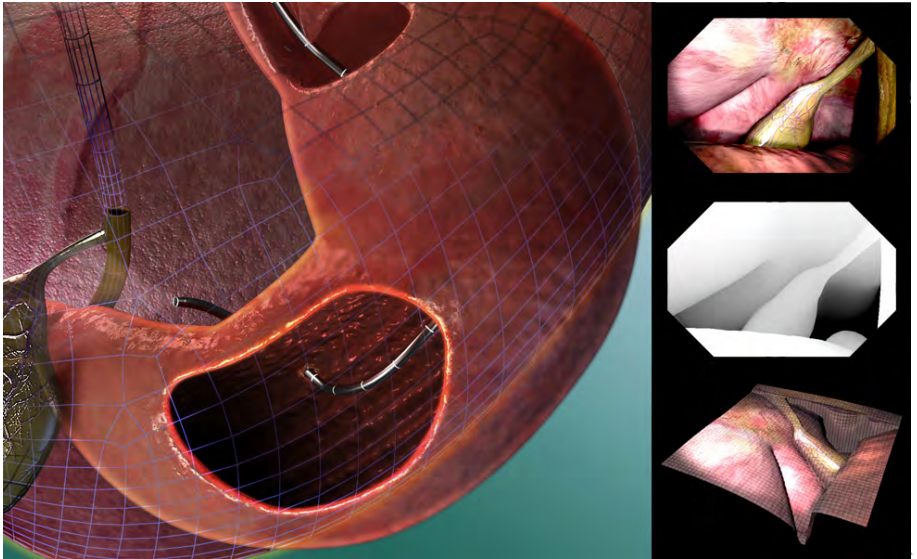
Finding the entry point to the peritoneal cavity





# Navigation support - Collision prevention

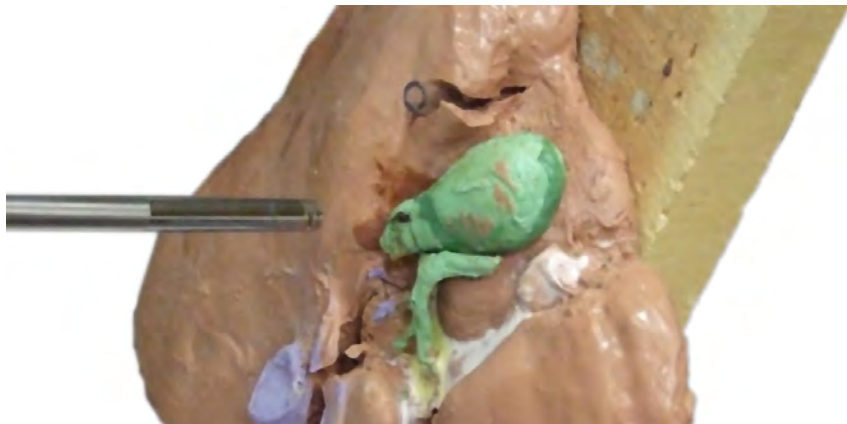
Finding the entry point to the peritoneal cavity





# Preliminary results

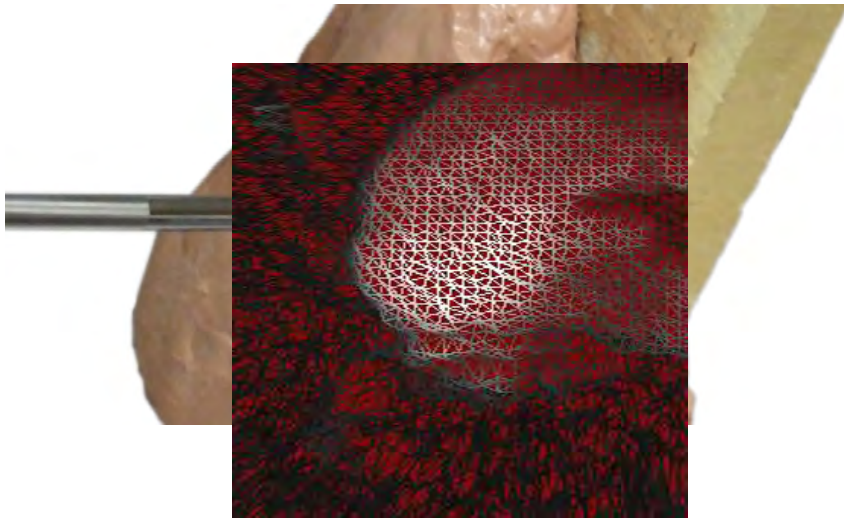
Liver phantom with gall bladder





# Preliminary results

Liver phantom with gall bladder

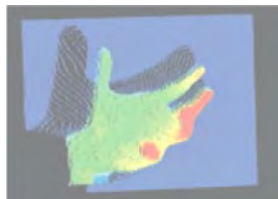






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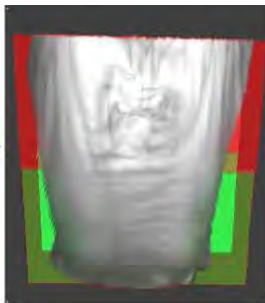


# ToF respiratory motion gating

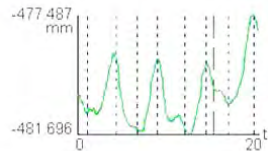
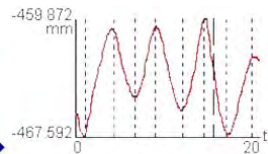
Thorax and Abdomen



**Aquisition**  
(Thorax / Abdomen)



**Preprocessing**  
(Thorax / Abdomen)

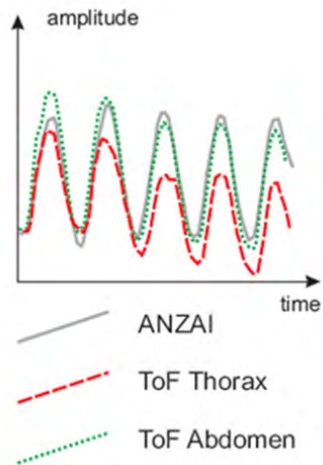
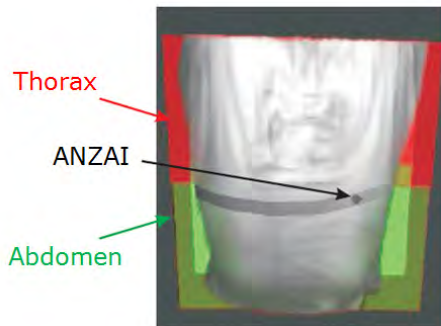


**Realtime Signal**  
(Thorax / Abdomen)



# ToF respiratory motion gating

## Evaluation





# ToF respiratory motion gating

## Evaluation



PET Scanner

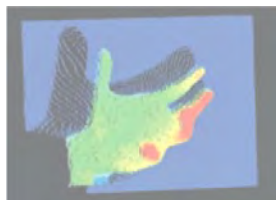


Lab Setup



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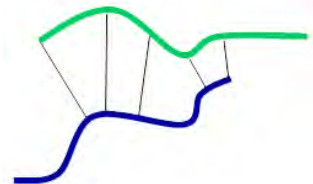
# ToF patient positioning

## Segmentation and registration

Segmentation



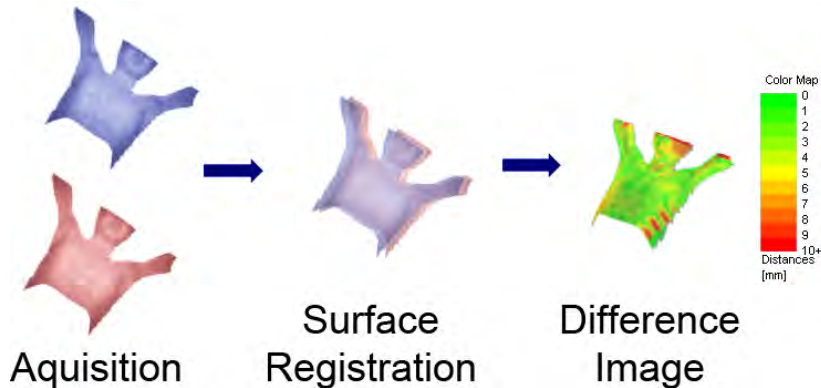
Registration





# ToF Patient Positioning

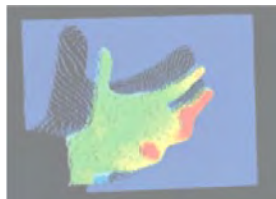
## Difference Image





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# Conclusion

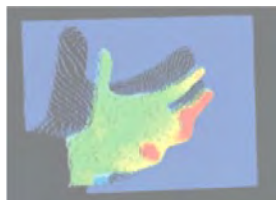
ToF cameras are off-the-shelf technology.

- 3-D endoscopy to provide an enhanced field of view and real-time collision prevention
  - Getting online distance information and computing off-axis view or reconstructed area by stitching
- ToF sensor for respiratory motion gating
  - Competitive approach improving PET, 4-D CT,...
- Patient positioning using 3-D surface registration
  - Adaption of preoperative CT planning in radiotherapy



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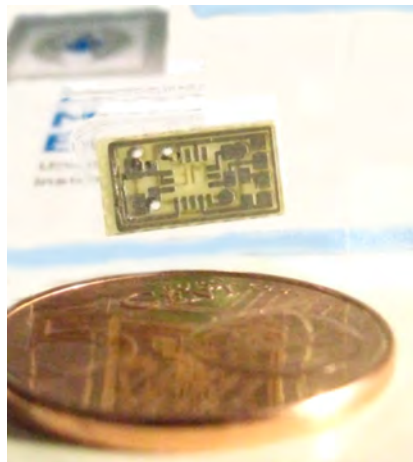


# Outlook

## Solution for loss of spatial orientation

Real-time information of spatial orientation by measuring gravity

- using MEMS-based inertial devices:  
3-D accelerometers





# The End

- Thank you for your attention!
- Any further questions?

