Dimensionality Reduction Techniques for Statistical Analysis and Modeling in Medical Imaging

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Agenda

- Introduction
 - Dimensionality Reduction
 - Statistical Analysis and Modeling
 - Nomenclature
- Linear Dimensionality Reduction
 - Principal Component Analysis (PCA)
 - Multidimensional Scaling (MDS)
 - Applications
- Non-linear Dimensionality Reduction
 - Kernel Principal Component Analysis (KPCA)
 - Manifold Learning and Graph-Based Methods
 - Applications



Motivation

- Dimensionality Reduction
- Statistical Analysis and Modeling
- Nomenclature





Dimensionality Reduction

- Curse of dimensionality
 - No statistical significance due to sparse sampling
 - Distance metrics not meaningful
 - Computational burden
- Visualization
 - Intuitive feel what the data looks like
 - Analysis of machine learning algorithms
- Underlying forces
 - How are samples created?
 - Important features and structures
 - Removal of misleading features





Statistical Analysis and Modeling

- Statistical analysis
 - Describe, understand and predict a population based on sample datasets (inference)
 - Characterize data in a short and compact form
 - Out-of-sample problem
- Statistical modeling
 - Reconstruction of a complex entity from a compact statistical description
 - Pre-image problem

Underlying statistical model?





Nomenclature

High-dimensional (mean-centered) input points

$$\left\{oldsymbol{x}_i
ight\}_{i=1}^n\;,\;oldsymbol{x}_i\in\mathbb{R}^D\;,\;\sum_ioldsymbol{x}_i=oldsymbol{0}$$

Low-dimensional output points

$$\mathbf{y}_i \in \mathbb{R}^d$$
, $d \ll D$

Matrix notation

$$oldsymbol{X} = [oldsymbol{x}_1, \dots, oldsymbol{x}_n] \in \mathbb{R}^{D imes n}$$

Inner products

$$oldsymbol{x}_i^ op oldsymbol{x}_j = \langle oldsymbol{x}_i, oldsymbol{x}_j
angle = (oldsymbol{x}_i \cdot oldsymbol{x}_j)$$





Nomenclature

- Out-of-sample problem
 - For an **unseen** sample $\hat{x} \in \mathbb{R}^D$, $\notin \{x_i\}_{i=1}^n$ what is its corresponding low-dimensional representation $\hat{y} \in \mathbb{R}^d$?
 - This may be a non-trivial task...
- Pre-image problem
 - Given an **arbitrary** low-dimensional representation $\widehat{\boldsymbol{y}} \in \mathbb{R}^d$, what is the corresponding vector $\widehat{\boldsymbol{x}} \in \mathbb{R}^D$ in input space?
 - For many dimensionality reduction techniques, the exact pre-image simply does not exist!



Linear Dimensionality Reduction

- Principal Component Analysis (PCA)
- Multidimensional Scaling (MDS)
- Applications





- Find the directions (i) along which the data has maximum variance and (ii) the relative importance of these directions
- Minimum reconstruction error:

$$\mathcal{J}_{ ext{PCA}} = \sum_{i} \left\| oldsymbol{x}_i - \sum_{j=1}^{d} \left(oldsymbol{x}_i \cdot oldsymbol{e}_j
ight) oldsymbol{e}_j
ight\|^2 = \sum_{i} \left\| oldsymbol{x}_i - oldsymbol{E} oldsymbol{y}_i
ight\|^2$$
 subject to $(oldsymbol{e}_i \cdot oldsymbol{e}_j) = \left\{ egin{array}{l} 1, & i = j \\ 0, & i
eq j \end{array}
ight.$

Solution given by Eigen-decomposition of the covariance matrix

$$oldsymbol{C} = rac{1}{n} \sum_i oldsymbol{x}_i oldsymbol{x}_i^ op = oldsymbol{E} oldsymbol{\Lambda} oldsymbol{E}^ op$$
, $oldsymbol{\Lambda} = diag\left(\lambda_1, \ldots, \lambda_D
ight)$





- Out-of-sample problem
 - ullet Principal axes $oldsymbol{E}$ derived from the training set $\left\{oldsymbol{x}_i
 ight\}_{i=1}^n$
 - For an unseen sample $\widehat{m{x}} \in \mathbb{R}^D$ its low-dimensional representation is:

$$\widehat{m{y}} = m{E}^{ op} \widehat{m{x}}$$

- Pre-image problem
 - ullet For an arbitrary low-dimensional representation $\widehat{m{y}} \in \mathbb{R}^d$ the corresponding vector in input space is

$$\widehat{x} = E\widehat{y}$$

ullet This follows from the orthonormality of E

This is straight-forward...





- PCA requires the data to lie on a d-dimensional linear subspace
 - This will introduce some error in practice
 - Will definitely fail for curved manifolds

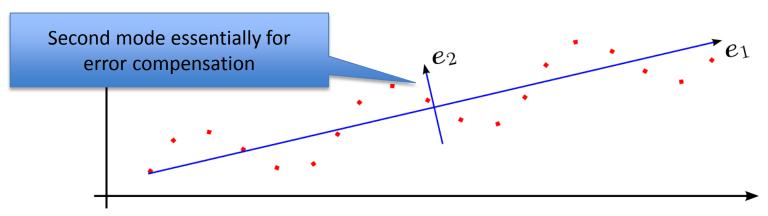


Figure: PCA applied to samples drawn from a sine curve.





- PCA yields global modes of variation
 - Sparsity is sacrificed for the sake of variance maximization
 - Remedies: Factor-Rotations [1], Sparsity-Regularization [2,3]

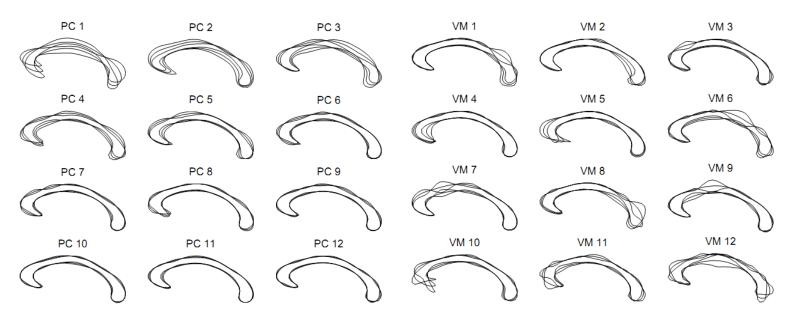


Figure: PCA and varimax rotations applied to corpus callosum annotations [1].





Multidimensional Scaling (MDS)

- Compute low-dimensional representation that preserves mutual inner products
 - Pairwise distances (equals PCA)
 - Mutual angles
 - Generalized metrics
- Objective function

$$\mathcal{J}_{ ext{MDS}} = \sum_{i,j} ig(oldsymbol{x}_i \cdot oldsymbol{x}_j - oldsymbol{y}_i \cdot oldsymbol{y}_jig)^2$$

Solution given by spectral decomposition of the Gram matrix

$$G_{i,j} = \boldsymbol{x}_i \cdot \boldsymbol{x}_j$$





 Statistical shape models for 3D medical image segmentation

On the one hand, the PCA approach employed by the vast majority of studies unquestionably has its weaknesses: A number of modeled shapes will certainly not feature Gaussian distributions and the linear approximation model will be suboptimal. On the other hand, PCA is fairly robust to the input data distribution and generally just works.

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Statistical shape models for 3D medical image segmentation: A review

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ARSTRACT

Statistical shape models (SMM) have by now been firmly established as a robust tool for regimentation of medical images, while 20 models have been in use tractile the adv 1900s, wide-spread will ration of three-dimensional models appeared only in recent years, primarily made possible by breakthrough in automatic detection of shape correspondences. In this strictle, we review the techniques regiment to create a deep many three 20 SMMs. While we concentrate on landmark-based shape representations and throughly examine the most popular variants of 64-rise Shape and Activate Appearance models and electric services and extensive services of the control state of the art in the field. We conclude with a survey of accidence and a discussion of future development.

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1. Introduction

In the last two decades, model-based segmentation approaches have been established as one of the most successful methods ro image analysis. By marching a model which contains information about the expected shape and appearance of the structure of interest to new images, the segmentation is conducted in a top-down fashion. Due to the inherent a-priori information, this approach is more stable against local image artifacts and perturbations than conventional low-level algorithms. While a single template shapes and advantage model for industrial applications where mass-produced, rigid objects need to be detected, this method is prone to fall in case of biological objects due to their considerable natural arability. Information about common variations thus has to be defined in the model. A straight-floward approach to gather this is to examine a number of training shapes by statisting of statistical shape models (SSMs).

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concentrate on methods for volumetric images. However, many modeling methods have only been applied to 2D so far. To the extent that such methods can be generalized or extended to the 3D case, we have included them in the present review. We have furthermore included some methods which have shown to be very successful in 2D, but which are technically not feasible in 3D – simply to emphasize the difference.

The objective of this article is to provide the reader with a summary of the current state of the art with regard to 3D statistical shape models, to demonstrate what has been done until now, but also to present some ideas of what might yet be done. To ensure comprehensive coverage, we have screened all publications in cluded in IEEE Transactions on Medical Imaging and Medical Image Analysis during the last 10 years for articles related to shape models. In addition, we have included a large number of articles from other international journals, but also numerous conference and workshop papers which present good ideas, but which have not been published in any journal yet. Our main source of references was the Internet; we have searched for the terms shape model and statistical model on PubMed IEEE-Xnlore Citeseer and Google We have also followed the references encountered in papers from these sites, until we had collected a comprehensive library of more than 400 articles on the topic. In case we encountered several papers from one author about the same subject, we generally picked the most detailed one for this review.

1.1 Paloted wor

Before reviewing statistical shape models, let us first define what we regard as related work that will not be discussed further in this article.

Heimann T, Meinzer HP.

Statistical shape models for 3D medical image segmentation: A review

In: Medical Image Analysis. Vol. 13(4), pp. 543-563, 2009





Model-based segmentation

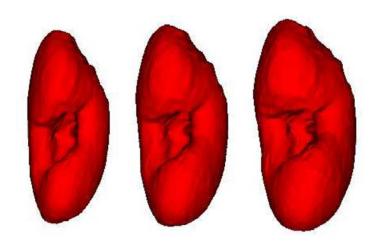
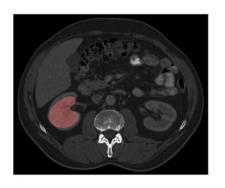
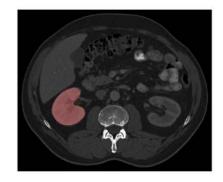


Figure: First mode of variation.





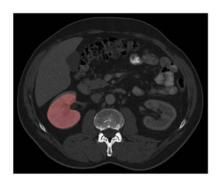




Figure: Kidney segmentation using ASMs.

Spiegel M, Hahn D, Daum V, Wasza J, Hornegger J.

Segmentation of kidneys using a new active shape model generation technique based on non-rigid image registration
In: Computerized Medical Imaging and Graphics. Vol. 33, pp. 29-39, 2009





4-D shape priors for respiratory motion management

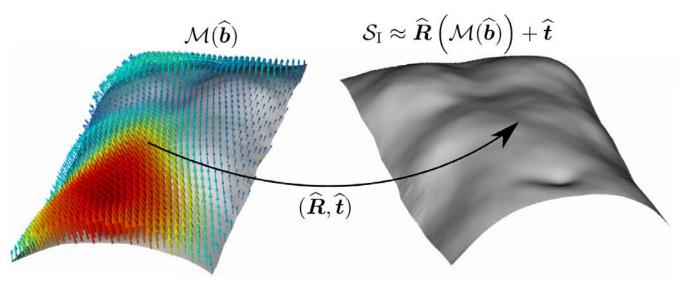


Figure: Motion compensated patient positioning

Wasza J, Bauer S, Hornegger J.

Real-time Motion Compensated Patient Positioning and Non-Rigid Deformation Estimation using 4-D Shape Priors
In: MICCAI 2012, accepted for publication





Respiratory model of anatomical motion

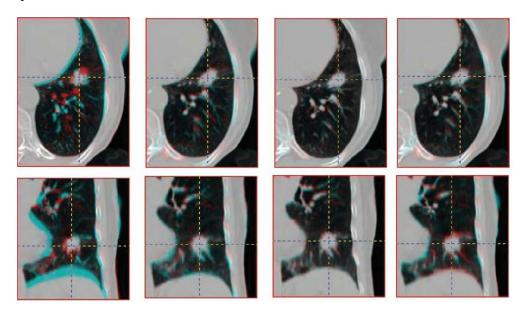


Figure: Actual CT and reconstructed volume.

Zhang Q, Pevsner A, Hertanto A, Hu Y, Rosenzweig K, Ling C, Mageras G. A patient-specific respiratory model of anatomical motion for radiation treatment planning In: Medical Physics. Vol. 34(12), pp. 4772-4781, 2007



Non-linear Dimensionality Reduction

- Kernel Principal Component Analysis (KPCA)
- Manifold Learning and Graph-Based Methods
- Applications





- Basic idea [4]: compute PCA in a **feature space** $\phi(x_i) \in \mathcal{H}$ instead of the original input space $x_i \in \mathbb{R}^D$
 - In general: $\mathcal{H} = \mathbb{R}^{\infty}$
 - Kernel trick: $\phi(\boldsymbol{x}_i) \cdot \phi(\boldsymbol{x}_j) = k(\boldsymbol{x}_i, \boldsymbol{x}_j)$
- Covariance matrix in feature space H

$$oldsymbol{C} = rac{1}{n} \sum_{i} \phi\left(oldsymbol{x}_{i}
ight) \phi\left(oldsymbol{x}_{i}
ight)^{ op}$$

- This is equivalent to non-linear MDS
 - Kernel matrix contains generalized inner products in feature space
 - Spectral decomposition of the Gram matrix in feature space





• Eigendecomposition of the kernel matrix ${m K}_{i,j} = k\left({m x}_i, {m x}_j\right)$

$$egin{aligned} oldsymbol{K} &= oldsymbol{E}oldsymbol{\Lambda}oldsymbol{E}^ op &= oldsymbol{E}oldsymbol{\Lambda}^{rac{1}{2}} \left(oldsymbol{E}oldsymbol{\Lambda}^{rac{1}{2}} \left(oldsymbol{E}oldsymbol{\Lambda}^{rac{1}{2}}
ight)^ op \ oldsymbol{E} &= \left[oldsymbol{e}_i, \ldots, oldsymbol{e}_n
ight] \;,\; oldsymbol{\Lambda} = diag\left(\lambda_1, \ldots, \lambda_n
ight) \end{aligned}$$

- Note that the number of modes equals the number of samples! This is in contrast to conventional PCA.
- Projection on the p-th Eigenvector ${m V}^p$

$$oldsymbol{y}_{i}^{p} = oldsymbol{V}^{p} \cdot \phi\left(oldsymbol{x}_{i}
ight) = \sqrt{\lambda_{p}} oldsymbol{e}_{i}^{p}$$

• Note that we assume the data to be mean-centered in feature space. This in general not valid, for details see [4].





- Out-of-sample problem
 - Not as easy as with conventional PCA
 - Related to the Nyström extension [5]

$$\widehat{\boldsymbol{y}}^{p} = \boldsymbol{V}^{p} \cdot \phi\left(\widehat{\boldsymbol{x}}\right) = \frac{1}{\sqrt{\lambda_{p}}} \sum_{i=1}^{n} \boldsymbol{e}_{i}^{p} \left(\phi\left(\boldsymbol{x}_{i}\right) \cdot \phi\left(\widehat{\boldsymbol{x}}\right)\right) = \frac{1}{\sqrt{\lambda_{p}}} \sum_{i=1}^{n} \boldsymbol{e}_{i}^{p} k\left(\boldsymbol{x}_{i}, \widehat{\boldsymbol{x}}\right)$$

- Pre-image problem
 - In feature space like regular PCA
 - From feature space to input space an ill-posed problem
 - Usually approximated by minimizing an error function [5]

$$\widehat{\boldsymbol{x}} = \underset{\boldsymbol{x}}{\operatorname{argmin}} \| \boldsymbol{V} \phi(\boldsymbol{x}) - \widehat{\boldsymbol{y}} \|^2$$





- Choosing the kernel function
 - Radial basis functions (RBF)
 - Polynomial kernels
 - Linear functions
 - See also Kernel-SVM and Kernel-SVR
- Parameters
 - Highly depend on the problem
 - Slightly different parameters usually produce complete different results

There is no rule which kernel to choose and how to select its parameters!





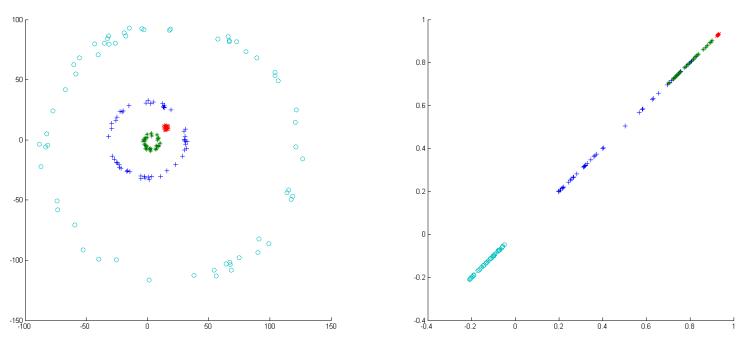


Figure: Dimensionality reduction using KPCA.





Manifold Learning and Graph-Based Methods

- Basic idea: duplicate the behavior of PCA on manifolds instead of linear subspaces
- Manifolds:
 - Low-dimensional structure embedded in a high-dimensional space
 - Geodesic distances vs. euclidean distances

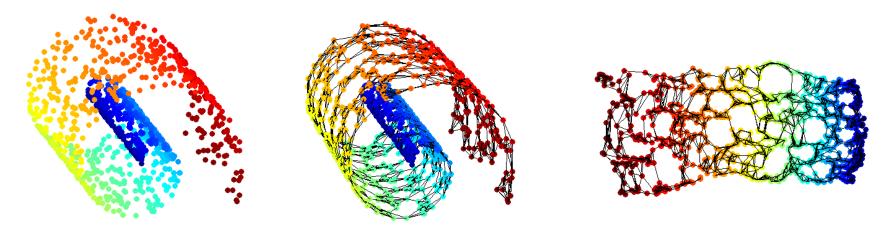


Figure: The swissroll manifold. Left: original data. Middle: connected data. Right: unfolded.





Manifold Learning and Graph-Based Methods

- Multitude of approaches (see [6,7] for overviews)
 - Isomap
 - Locally Linear Embedding
 - Laplacian Eigenmaps
 - Maximum Variance Unfolding
 - ...
- Key issues
 - Discrete manifold approximations (graphs)
 - Geodesic distances (shortest paths)





Manifold Learning: Isomap

- Idea: Preserve distances between input patterns as measured along the manifold from which they were sampled —> Geodesic distances
- Estimation of geodesic distances
 - *k*-nearest neighbor graph $\mathcal{G}_k = (\mathcal{V}, \mathcal{E}_k)$

$$\mathcal{V} = \left\{oldsymbol{x}_i
ight\}_{i=1}^n \;, \, \mathcal{E}_k = \left\{\left\|oldsymbol{x}_i - oldsymbol{x}_j
ight\| \; \left\|oldsymbol{x}_j \in \mathcal{N}^k\left(oldsymbol{x}_i
ight)
ight\}$$

Geodesic distance matrix

$$D_{i,j} = \text{ShortestPath}\left(\mathcal{G}^k, \boldsymbol{x}_i, \boldsymbol{x}_j\right)$$

Classical MDS on the geodesic distances

$$\mathcal{J}_{\mathrm{IsoMDS}} = \sum_{i,j} (D_{i,j} - \boldsymbol{y}_i \cdot \boldsymbol{y}_j)^2$$





Manifold Learning and Graph-Based Methods

- Out-of-sample problem
 - Depends on the method
 - Often related to the Nyström extension
- Pre-image problem
 - Depends on the method
 - Closely related to the out-of-sample problem
- Common problems
 - All algorithms require a neighborhood size
 - Theoretical performance results often not available
 - Target dimensionality must be specified in general
 - Do real world data exhibit manifold structures?





Image-based breathing gating

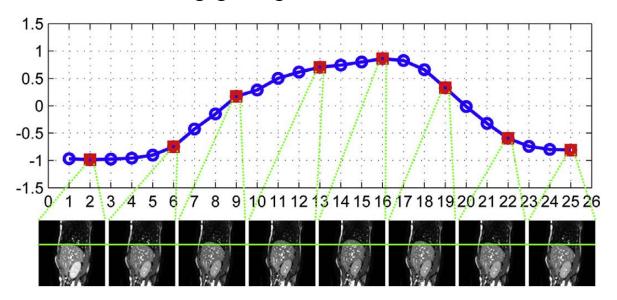


Figure: Image-based breathing signal obtained by manifold learning.

Wachinger C, Yigitsoy M, Rijkhorst E, Navab N.

Manifold learning for image-based breathing gating in ultrasound and MRI
In: Medical Image Analysis, Vol. 16(4), pp.806-818, 2012





Registration, Segmentation and Classification

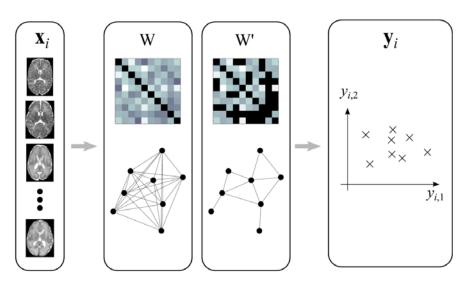


Figure: Schematic overview of manifold learning in medical imaging.

Aljabar, P, Wolz R, Rueckert D.

Manifold Learning for Medical Image Registration, Segmentation and Classification
In: Machine Learning in Computer-Aided Diagnosis: Medical Imaging Intelligence and Analysis, 2012





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