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## **Rectification of Endoscopic Images by Gravity**

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# Rectification of Endoscopic Images by Gravity

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**Abstract.** Image rotation correction even in non-rigid endoscopic surgery (particularly NOTES) can be realized with a tiny MEMS tri-axial inertial sensor placed on the tip of an endoscope by measuring the impact of gravity on each of the three orthogonal axes. After an initial calibration the rotation angle can be estimated with some calculations out of these three values. Achievable repetition rate is above the usual endoscopic video frame rate of  $30Hz$ , accuracy is about one degree. The image rotation was performed by rotating just digitally a capture of the endoscopic analogue video signal which can be realized in real-time. Improvements and benefits have been evaluated in animal studies: Coordination of different instruments and estimation of tissue behaviour regarding gravity related deformation and movement was considered to be much more intuitive having a stable horizon on endoscopic images.

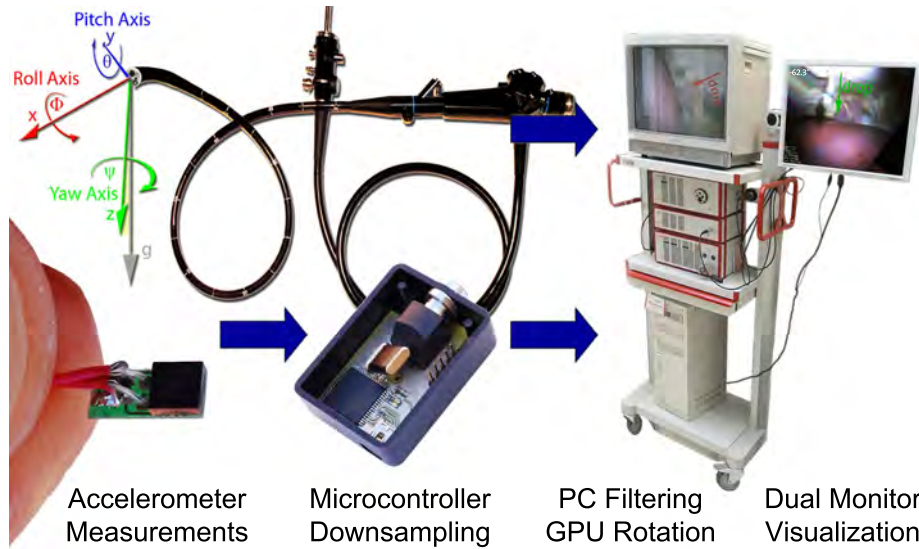
## 1 Method

One of the biggest problems with flexible endoscopy in Natural Orifice Transluminal Endoscopic Surgery (NOTES) [1] is the missing information about image orientation [2]. Thus, tip retro-flexion of a non-rigid endoscope causes image rotation angles till  $\pm 180$  degrees.

Our approach to measure this orientation angle is to integrate a Micro Electro-Mechanical System (MEMS) based inertial sensor device in the endoscope's tip, which measures influencing forces in three orthogonal directions [3,4]. If the endoscope is not moving, only the acceleration of gravity has an effect on the three axes. Using an arc tangent function the rotation angle  $\Phi$  can be computed out of acceleration values  $F_y$  and  $F_z$  on the two axes  $y$  and  $z$  orthogonal to the endoscopic line of view in  $x$ -direction:

$$\Phi = \arctan2(F_y, F_z) \quad (1)$$

First, a preceded  $3 \times 3$  calibration matrix, which incorporates misalignment and scaling errors [5], has to be retrieved by initial measurements. Moreover a peak elimination is the result of clever down sampling the measuring frequency, which is considerably higher than the image frame rate, using a weighted sum algorithm. To avoid bouncing or jittering images as a result of the angle correction, additional filtering is necessary.



**Fig. 1.** EndoSens Hardware with ENDOrientation Algorithm for Endoscopic Image Rectification

Hence, prior to angle calculation, the measures of each axis are filtered with a Hann filter to smooth angle changes and with a minimum variation threshold to suppress dithering.

With the employed sensor there is a uniform quantization of 8 bit for a range of  $\pm 2.3g$  for each axis. This implies a quantization accuracy of  $0.018g$  per step or 110 steps for the focused range of  $\pm g$ . This is high enough to achieve a durable accuracy even to a degree within relatively calm movements. This is possible as roll angle  $\Phi$  is calculated out of inverse trigonometric values of two orthogonal axes. Single extraordinary disturbed MEMS values or superposed accelerations with the same order of magnitude as gravity are suppressed by the ENDOrientation algorithm [6].

## 2 Results

During a porcine animal study, the navigation complexity of a hybrid endoscopic instrument during a NOTES peritoneoscopy with the well established trans-sigmoidal access [7] was compared with and without automated image rotation. To evaluate the benefit of automated real-time MEMS based image rectification, four different needle markers were inserted through the abdominal wall to the upper right, lower right, lower left and upper left quadrants. These four needle markers had to be grasped with a trans-abdominal introduced endoscopic needle holder under standardized conditions. The minimum time, the mean time and the maximum time have been lower with image rectification for every position [8]. All participating surgeons considered the complexity lower using our ENDOrientation technique.

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