# Image-based Compensation for Involuntary Motion in Weight-bearing C-arm CBCT Scanning of Knees

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**TECHNISCHE FAKULTÄT** 











- Knee-joint kinematics change under strain
  - In particular: different flexion angles
- Enable weight-bearing acquisitions
  - → Dedicated CBCT scanners
  - → Existing systems
- C-arm CT scanners
  - ightarrow Horizontal trajectories
  - ightarrow Wide volumetric beam coverage











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- Weight-bearing acquisitions:
  - ightarrow From standing upright through to deep squats (65° flexion)
- Involuntary knee motion during scans
  - ightarrow Severe motion artifacts
- Previously: Use of fiducial markers Compensation in:
  - Reconstruction space
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# Outline

- Review of the marker-based approach
- Introduction to the image-based approach
- Results
- Conclusions



# **Outline: Projection Shifting Algorithm**

- 1. Generate projections of the static 3D scene
  - Estimate static (mean) 3D position of features (e.g. markers)
  - Forward project the scene
- 2. Calculate projection shifts
- 3. Apply shifts and back-project







## **Marker-based Projection Shifting**



- Detect position  $(u, v)_i^{(j)}$  of marker i = 1, ..., N in projection j
- Calculate mean marker position  $(\bar{x}, \bar{y}, \bar{z})_i$  in 3D space

$(\Delta u, \Delta v)^{(j)T}$	$= \frac{1}{N} \sum_{i} \left( \mathbf{P}^{(j)} \cdot \bar{\mathbf{x}}_{i}^{T} - (u, v)_{i}^{(j)T} \right)$









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- Detect position  $(u, v)_i^{(j)}$  of marker i = 1, ..., N in projection j
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Calculate 2D shift:  $(\Delta u, \Delta v)^{(j)T} = \frac{1}{N} \sum_{i} \left( \mathbf{P}^{(j)} \cdot \bar{\mathbf{x}}_{i}^{T} - (u, v)_{i}^{(j)T} \right)$ 



## Use image registration to calculate 2D projection shifts.

- Estimate of motion-corrected projections
  - 1. FDK-type uncompensated reconstruction
  - 2. Gaussian smoothing
  - 3. Maximum-Intensity-Projections (MIPs) of the volume → MIPs dominated by high-intensity structures
- Calculate projection shifts  $(\Delta u, \Delta v)^{(j)}$ 
  - Registration of MIPs to motion-corrupted projections
     → Mutual information in 4 scale-space levels
- Shift and reconstruct



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# **Remarks on Mutual Information**

# How much information about **m** is contained in **f**

Mutual information

 $MI(m(\mathbf{x}), f(T(\mathbf{x}))) = H(m(\mathbf{x})) + H(f(T(\mathbf{x}))) - H(m(\mathbf{x}), f(T(\mathbf{x})))$ 

- Marginal and joint entropy: H(y), H(y, z)
- Calculated from histograms: Parzen Window approximation
- $\rightarrow$  No explicit form of dependency needed. But the histograms must be "related".









## **Procedure**



# Perform FDK-type reconstruction → Modeling clay to avoid detector saturation









## **Procedure**



• Calculate MIPs and register to acquisitions  $\rightarrow$  Note clay artifact in MIPs









### **Experiments:**

- Five healthy volunteers imaged
- Standing upright, 35° and 65° flexion
- $\rightarrow\,$  Two scans with significant motion artifact shown Scan A at 35° and Scan B at 65° flexion

## Evaluation:

- Qualitatively: visual inspection
- Quantitatively: marker-based results (gold standard)









## **Results: Scan A**



Error: 2.89  $mm \pm 1.24 mm$  (uncorrected: 3.50  $mm \pm 1.90 mm$ )









## **Results: Scan A**





#### Uncompensated reconstruction

Proposed method









## Remarks



- Both knees "aligned"
- Boundaries in *u*-direction pronounced
- Boundaries in *v*-direction suppressed (artifact)
- Structures resulting from overlap not present in MIPs
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## **Results: Scan B**



Error: 2.90  $mm \pm 1.43 mm$  (uncorrected: 4.10  $mm \pm 3.03 mm$ )









## **Results: Scan B**





#### Uncompensated reconstruction

Proposed method



## **Observations**

Mean error after correction remains significant in both scans.

#### Can we get better with iterative application of the method?

Iterative application did not help with the current pipeline.

Possible reasons:

- Using MIPs as reference projections is not optimal
- Mutual information cannot handle the given problem









### Performance w.r.t. Marker-based Method



#### Figure: Uncompensated, proposed and marked-based reconstructions



## **Discussion and Conclusion**

#### Motion must be visible in high-intensity structures

 $\rightarrow$  Biased registration in the presence of artifacts (modeling clay)

#### Stable registration remains challenging

- MIPs & acquisition: dissimilar intensity range and appearance
- $\rightarrow$  Best similarity metric?
- $\rightarrow$  Use iterative reconstruction and integrated projections?

#### 3D motion compensation using 3D/2D registration

# First step towards automatic image-based motion compensation for weight-bearing knee imaging



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