Convex Temporal Regularizers in Cardiac C-arm CT

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Clinical Setting

- Interventional 4-D (3-D+t) C-arm CT of heart chambers
- Goal: Analysis of cardiac function



Fig.: Artis zeego multi-axis C-arm system, Siemens Healthcare GmbH, Forchheim, Germany.



Fig.: Rotational angiogram, courtesy of Dr. Gregor Krings, University Medical Center Utrecht, Netherlands.

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Gated Reconstruction

Retrospective electrocardiography (ECG) gating [1]:



Fig.: Projection images from a C-arm sweep belonging to the same relative heart phase.

[1] Desjardin et al.: ECG-gated Cardiac CT, Am J Roentgenol, 2004



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4-D Reconstruction

- Strong angular undersampling of individual phases
- But: Short scan available (albeit inconsistent)
 - Motion compensation [1,2]
 - Static guidance image for regularization [3]
 - Temporal smoothing / regularization [2,4]

[1] Müller et al.: Image artefact propagation in motion estimation and reconstruction in interventional cardiac C-arm CT, *PMB*, 2014

[2] Taubmann et al.: Coping with real world data: Artifact reduction and denoising for motion-compensated cardiac C-arm CT, *Med Phys*, 2016

[3] Chen et al.: **Prior image constrained compressed sensing (PICCS): A method to accurately reconstruct dynamic CT images from highly undersampled projection data sets**, *Med Phys*, 2008

[4] Mory et al.: Cardiac C-arm computed tomography using a 3D + time ROI reconstruction method with spatial and temporal regularization, *Med Phys*, 2014



Gated Iterative Reconstruction

- 1. Assign data to phases $t \in \{1, 2, \dots, N_{\text{phases}}\}$
- 2. Initialize $I^t = 0$
- 3. Main loop
 - i. SART update
 - ii. Spatial total variation (TV) reduction
 - iii. One of three convex temporal regularizers:

Temporal Rank-	Temporal Total Variation	Temporal Tight Frame
Regularization	Regularization	Regularization



Temporal Rank-Reducing Regularization

- Phases I^t not independent
 - Same object in different states
 - Underlying variation governed by few components
- Simplified assumption of few linear components:

$$I^{t_i} = a \cdot I^{t_j} + b \cdot I^{t_k} + \cdots$$

- Principle: Rank reduction
 - But: Rank constraint yields NP-hard reconstruction problem
 - Best convex approximation \rightarrow nuclear norm (sum of singular values)



Temporal Rank-Reducing Regularization

• Images arranged column-wise in a matrix

 $oldsymbol{I} = [oldsymbol{I}^1, oldsymbol{I}^2, \dots, oldsymbol{I}^{N_{ ext{phases}}}] \in \mathbb{R}^{N_{ ext{voxels}} imes N_{ ext{phases}}}$

• "Closest" images with reduced nuclear norm $\|\cdot\|_*$

$$\operatorname{prox}_{\|\|_{*},\lambda_{NN}}(\boldsymbol{I}) = \operatorname{argmin}_{\boldsymbol{I}'} \frac{1}{2} \|\boldsymbol{I} - \boldsymbol{I}'\|_{F}^{2} + \lambda_{NN} \|\boldsymbol{I}'\|_{*}$$

• Closed-form solution using SVD $I = U \Sigma V^{\top}$ and "soft thresholding"

$$\boldsymbol{I} \leftarrow \boldsymbol{U}(\boldsymbol{\Sigma} - \boldsymbol{1} \cdot \lambda_{NN})_{+} \boldsymbol{V}^{\top}, \qquad (\cdot)_{+} \equiv \max(\cdot, 0)$$



Temporal Total Variation (tTV) Regularization

- Medical images as cartoons (piecewise constant)
 - Ideal model: Reduce "jumps," i.e. L⁰ pseudo-norm of gradient
 - In practice: L^1 norm as its convex envelope (\rightarrow total variation)
- Natural extension to temporal dimension:





Temporal Total Variation (tTV) Regularization

• Temporal gradient (forward differences) as sparsifying transform

$$\mathcal{D}_t \boldsymbol{I} = [\boldsymbol{I}^2 - \boldsymbol{I}^1, \boldsymbol{I}^3 - \boldsymbol{I}^2, \dots, \boldsymbol{I}^1 - \boldsymbol{I}^{N_{ ext{phases}}}]$$

• Iterative descent along negative gradient of TV norm w.r.t. image

$$-\frac{\partial}{\partial I} \|I\|_{tTV} = -\frac{\partial}{\partial I} \|\operatorname{vec}(\mathcal{D}_t I)\|_1 \quad \text{(approx. by "corner rounding")}$$

• Convex combination of result $I_{\rm tTV}$ to control trade-off

$$\boldsymbol{I} \leftarrow \boldsymbol{I} + \lambda_{\text{tTV}} \left(\boldsymbol{I}_{\text{tTV}} - \boldsymbol{I} \right)$$



Temporal Tight Frame (TF) Regularization

- Wavelet-based sparsifying transform as a popular alternative
- Decompose, reduce high-frequency energies, recompose:





Temporal Tight Frame (TF) Regularization

• Piecewise linear tight frame

$$m{h}_0 = rac{1}{4}[1,2,1], \ m{h}_1 = rac{\sqrt{2}}{4}[1,0,-1], \ m{h}_2 = rac{1}{4}[-1,2,-1]$$

Convolution along temporal dimension

$$C = WI = \{C_i : C_i = h_i *_t I\}$$

• Reduction of high-pass energies $\|C\|_{ ext{TF}}$

$$\|\boldsymbol{C}\|_{\mathrm{TF}} = \|\operatorname{vec}(\sum_{i=1}^{2} (\boldsymbol{C}_{i})^{2})^{\frac{1}{2}}\|_{1}$$



Temporal Tight Frame (TF) Regularization

• "Closest" coefficient images with reduced $\|C\|_{ ext{TF}}$

$$\operatorname{prox}_{\|\|_{\mathrm{TF}},\lambda_{\mathrm{TF}}}(\boldsymbol{C}) = \operatorname{argmin}_{\boldsymbol{C}'} \sum_{i=0}^{2} \frac{1}{2} \|\boldsymbol{C}'_{i} - \boldsymbol{C}_{i}\|_{\mathrm{F}}^{2} + \lambda_{\mathrm{TF}} \|\boldsymbol{C}'\|_{\mathrm{TF}}$$

Closed-form solution ("vector shrinkage")

$$\boldsymbol{C}_{i,j}^t \leftarrow \begin{cases} \boldsymbol{C}_{i,j}^t & \text{if } i = 0, \\ \boldsymbol{C}_{i,j}^t \cdot \left(1 - \lambda_{\mathrm{TF}} \cdot \left(\sum_{i=1}^2 (\boldsymbol{C}_{i,j})^2\right)^{-\frac{1}{2}}\right)_+ & \text{else} \end{cases}$$

• Update step

$$\boldsymbol{I} \leftarrow \boldsymbol{W}^{-1} \operatorname{prox}_{\|\|_{\mathrm{TF}}, \lambda_{\mathrm{TF}}}(\boldsymbol{W}\boldsymbol{I})$$



Data

- Dynamic heart phantom data set [1,2]
 - Projections simulated using polychromatic X-ray spectrum
 - Ground truth reconstruction from projections of static phantom
 - 10 heartbeats
- Clinical patient data set
 - 13 heartbeats (140 bpm through external pacing)
 - 133 projection images (5 s scan, approx. 30 Hz)
 - 8 phases, 256³ voxels (1.0 mm/voxel isotropic)

[1] Segars et al.: 4D XCAT phantom for multimodality imaging research, *Med Phys*, 2010
[2] Maier et al.: Fast Simulation of X-ray Projections of Spline-based Surfaces using an Append Buffer, *PMB*, 2012



Evaluation

- Phantom study (quantitative, qualitative)
 - RMSE w.r.t. ground truth to assess convergence
 - Calculation restricted to ROI tightly enclosing the heart
 - Find "interesting" range of regularizer strength λ
- Clinical data (qualitative)
 - Similar behavior in real data? (aka: does it work?)
 - Is parameterization (somewhat) transferable?





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Results

350

300

250

200

150

100

0

0.2

0.4

 λ_{tTV}

RMSE w.r.t. Ground Truth / HU

- Higher λ : Faster start, earlier saturation
- TF, tTV: Similar values near optimum
- "Valley" more pronounced for TF
- Rank-regularization least effective, yet still better than none



x 10⁻³

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 λ_{TF}



Results





Results





Discussion

- Poor performance of variant with no temporal regularization
 - Massive angular undersampling (~10-13 distinct views per phase)
 - Challenging even for compressed sensing methods
- Mediocre results for rank-regularization
 - Linear model too simplistic for our use case
 - Possibly useful at early stage for outlier suppression?
- So, does TV reign supreme?
 - Most forgiving w.r.t. parameter choice
 - Synergy with spatial TV?
 - But: No closed-form solution of proximal operator



Conclusion

• Three temporal regularizers compared side-by-side:

Temporal Rank- RegularizationTemporal Total Variation Regularization	Temporal Tight Frame Regularization
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- Each better than spatial regularization only
- Varying levels of effectiveness and parameter sensitivity
- Similar behavior in phantom and real data (tentatively)
- Upcoming:
 - Convex optimization based on primal-dual splitting
 - Task-based assessment



Thanks for your attention!

Questions?









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