

Intuitive and Smart Editing of 3D Geometrical Heart Valve Models from Cardiac CT Data

Master Thesis Final Presentation

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January 26, 2015

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Outline

- Motivation
- Methods
- Implementation
- Results
- Outlook
- Summarization

Motivation

Fully automatic vs. manual segmentation

- fully automatic detection is not always reliable
- manual segmentation can be very time-consuming

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⇒ Solution: Intuitive and Smart Editing after fully-automatic initialization

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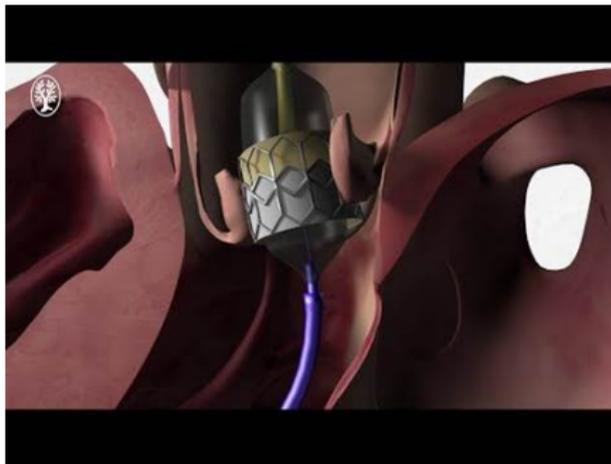
⇒ Solution: Intuitive and Smart Editing after fully-automatic initialization

Goals

- efficiency: faster than fully manual modeling
- interactivity: computations should not cause a delay
- intuitiveness: simple to apply, without knowing the mathematics
- robustness: result should be improved after each editing step

3D Geometric Aortic Valve Model

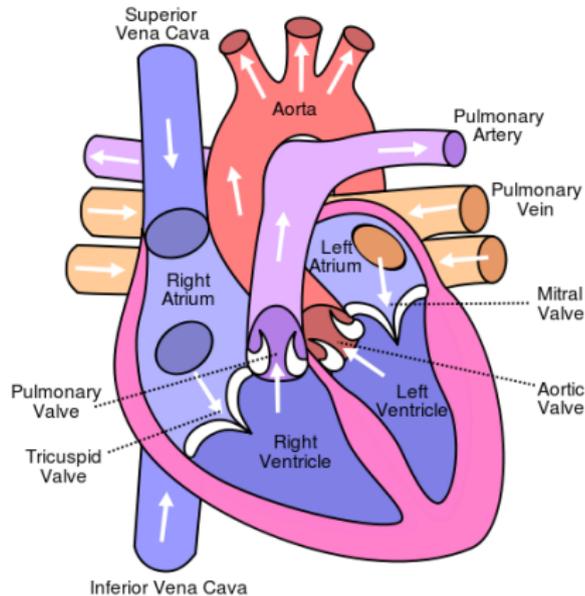
Purpose: diagnosis, surgery and therapy-planning



e.g. Transcatheter Aortic Valve Implantation (TAVI)

Methods

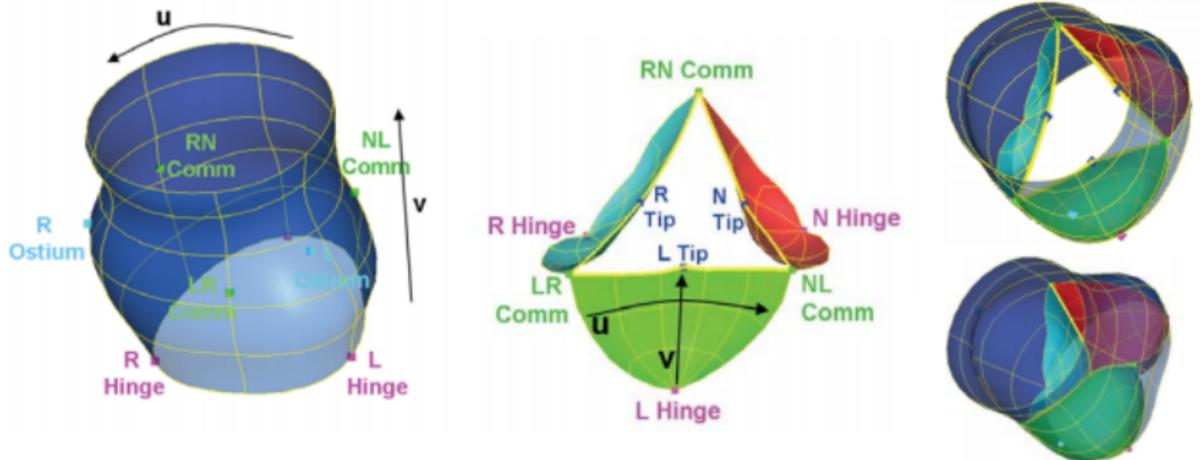
Medical Background: Anatomy of the Heart



Fully-automatic detection

Hierarchically defined physiological aortic valve model

1. Global location and rigid motion model
2. Nonrigid landmark motion model
3. Surface model



Local Surface Editing

- move one vertex \mathbf{v}_i to new position \mathbf{v}'_i
- vertices \mathbf{v}_j in neighborhood are moved in same direction $\mathbf{d} = \mathbf{v}'_i - \mathbf{v}_i$
- moving is damped by influence factor:

$$k_j = \frac{1}{2} \left(\cos\left(\pi \frac{\|\mathbf{v}_j - \mathbf{v}_i\|}{R}\right) + 1 \right)$$

- moving is damped by angle damping factor:

$$d_j = \cos(\angle(\mathbf{n}_j, \mathbf{n}_i)) = \mathbf{n}_j \cdot \mathbf{n}_i \quad (\mathbf{n}_i \text{ is vertex normal of } \mathbf{v}_i)$$

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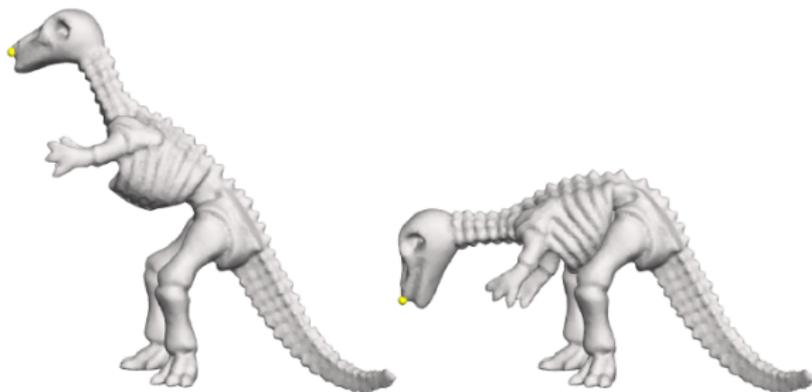
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⇒ new vertex positions: $\mathbf{v}'_j = \mathbf{v}_j + k_j d_j \mathbf{d}$

As-Rigid-As-Possible (ARAP) Surface Editing

- fix and move some constraints on the surface
- the remaining, free part of the surface is deformed physically plausible
- the global shape of the surface is preserved



ARAP Surface Editing

- \mathcal{N}_i : one-ring neighbors of v_i (all neighbors connected by an edge)
- R_i : rotation matrix

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SVD of Covariance matrix: $\mathbf{\Sigma}_i = \sum_{j \in \mathcal{N}_i} (\mathbf{v}_i - \mathbf{v}_j)(\mathbf{v}'_i - \mathbf{v}'_j)^T = \mathbf{U}_i \mathbf{S}_i \mathbf{V}_i^T$

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Best-aligning rotations: $R_i = \mathbf{V}_i \mathbf{U}_i^T$

ARAP: Objective function

$$E_{ARAP}(\mathbf{V}') = \sum_{i=1}^{|\mathcal{V}|} \sum_{j \in \mathcal{N}_i} \|(\mathbf{v}'_i - \mathbf{v}'_j) - \mathbf{R}_i(\mathbf{v}_i - \mathbf{v}_j)\|^2 \rightarrow \min$$

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Solve by iterative optimization

1. fix vertex-positions \mathbf{v}'_i , compute best-aligning rotations \mathbf{R}_i (as shown)
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$$\mathbf{L}\mathbf{V}' = \mathbf{B}$$

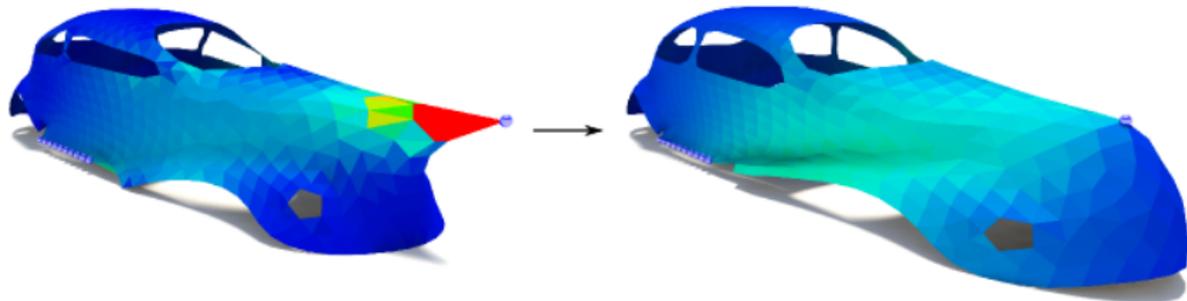
Smooth Energies for ARAP

- problem: artifacts at constrained positions
- good portion of ARAP energy is located at constraints
- when deformation contains stretching: peaks at constraints

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⇒ incorporate energy smoothness



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Use regularization parameter β :

$$E_{TOTAL}(\mathbf{V}') = (1 - \beta)E_{ARAP}(\mathbf{V}') + \beta E_{SMOOTH}(\mathbf{V}')$$

Implementation

Implementation

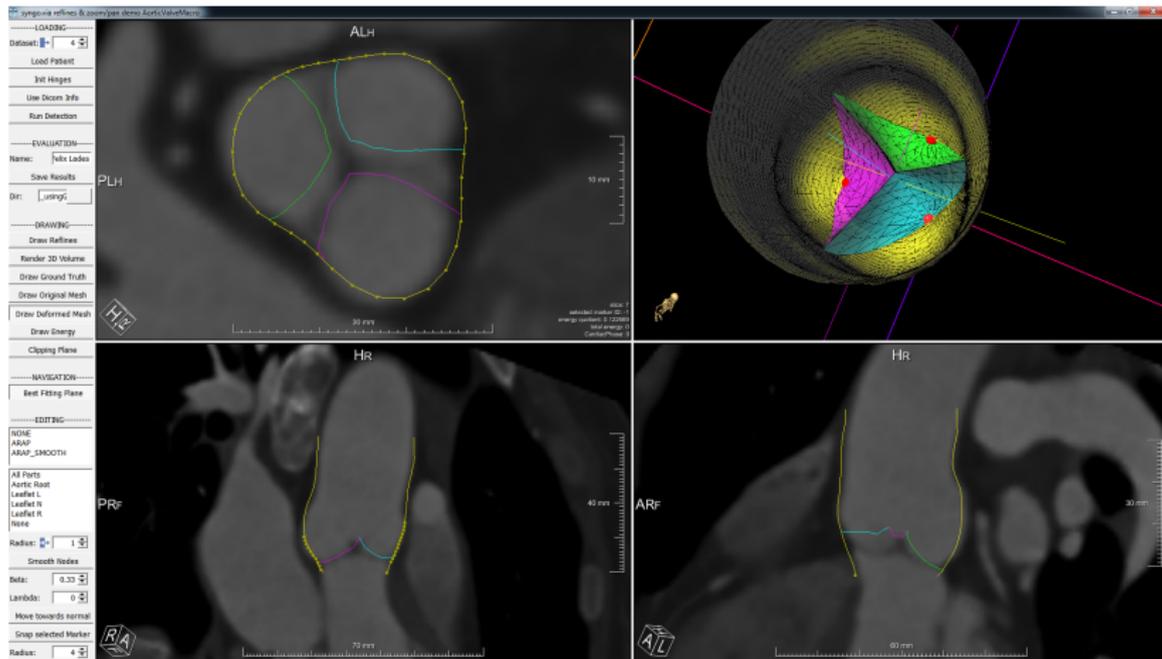
MeVisLab: platform to develop clinical prototypes

- modular C++ interface
- combine algorithms to pipelines and networks
- Open Inventor for interaction and 3D visualization

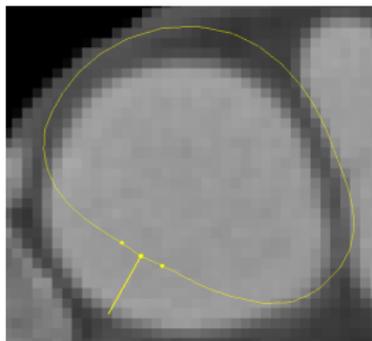
Eigen C++ template library for linear algebra

- Sparse matrix manipulations
- Solving sparse linear systems, e.g. Sparse Cholesky factorization
- SVD

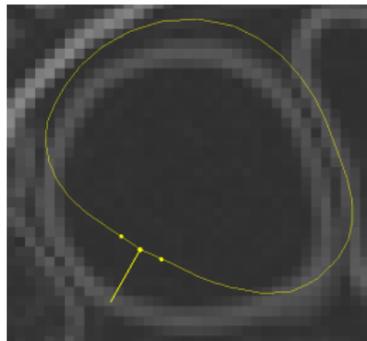
Prototype GUI



Edge snapping



Original image

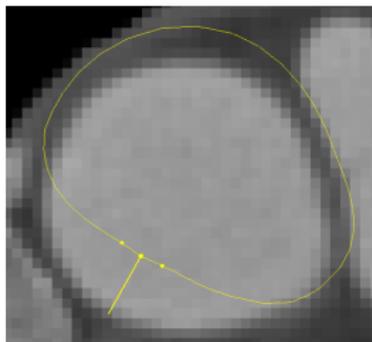


Gradient image

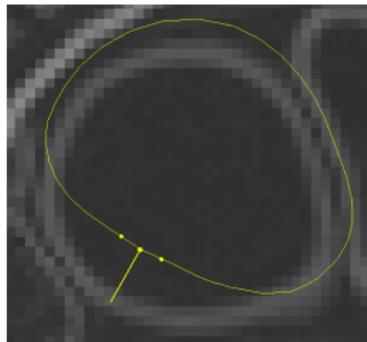


Illustration: voxel sampling

Edge snapping



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Gradient image

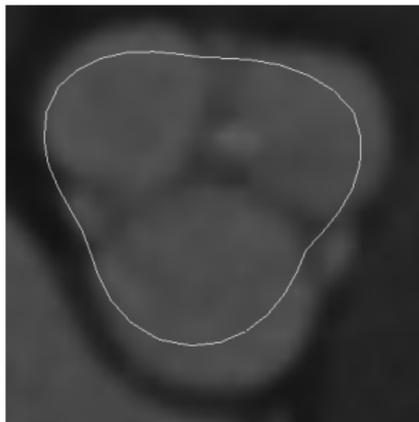


Illustration: voxel sampling

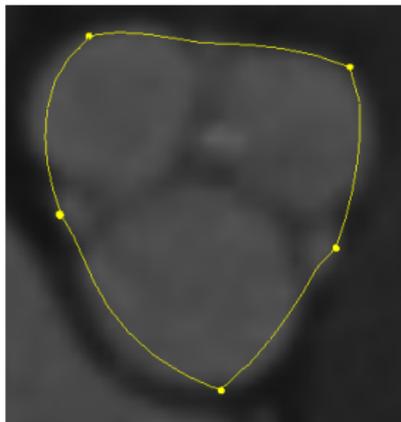
- moved vertex snaps into edge
- here: maximum gradient along moving direction
- highly extendable (e.g. higher level edge detection)

Results

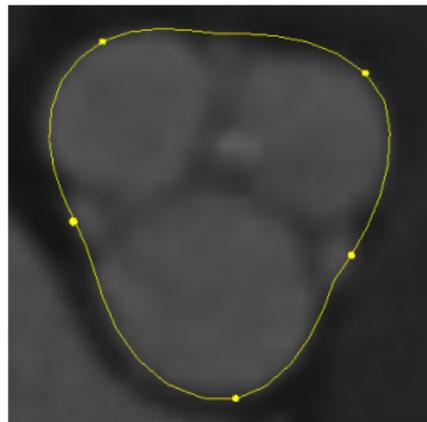
Energy Smoothness Regularization



Initialization with mean
shape model

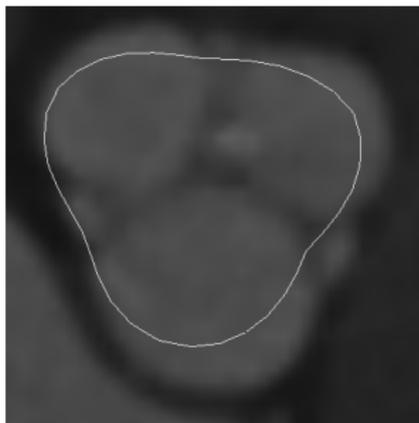


5 constraints, $\beta = 0$

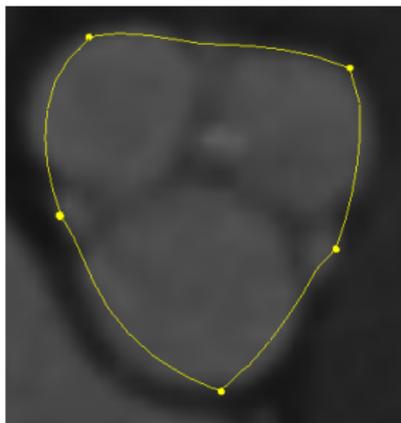


5 constraints, $\beta = 0.33$

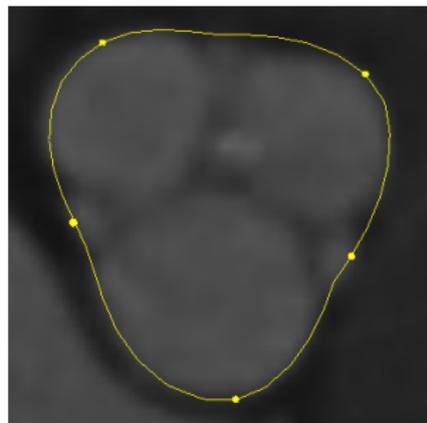
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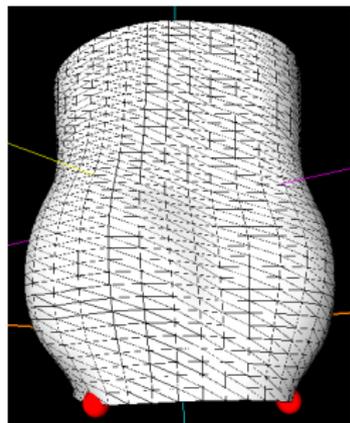
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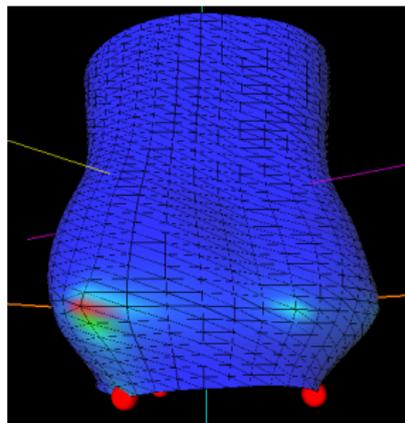
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⇒ smoother results with energy smoothness regularization

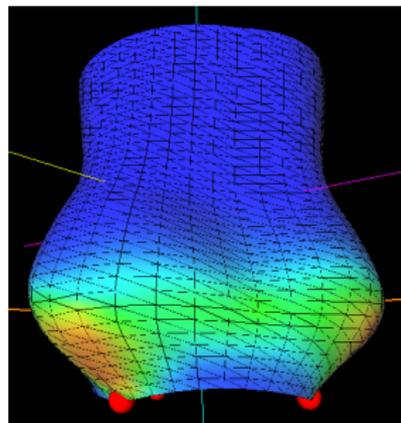
Energy Smoothness Regularization (energy color-coded)



Initialization with mean shape model



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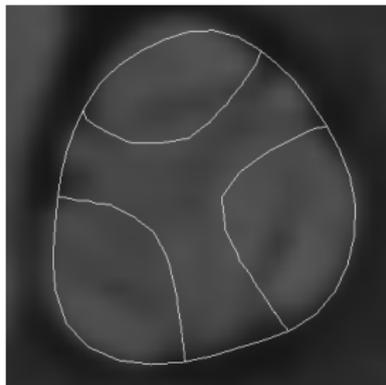
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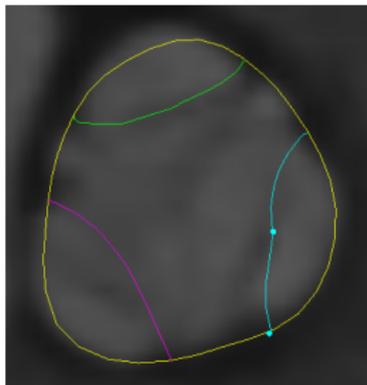
User study: editing of the aortic root

Data set	1	2	3	4	5	6
$d_{avg,init}$ [mm]	2.21	1.13	1.05	1.68	1.39	2.43
$d_{max,init}$ [mm]	6.40	3.41	3.80	4.29	4.43	12.10
$d_{avg,edit}$ [mm]	0.50	0.47	0.57	0.37	0.38	0.60
	± 0.07	± 0.05	± 0.04	± 0.03	± 0.02	± 0.15
$d_{max,edit}$ [mm]	2.04	2.25	1.82	1.84	1.98	2.43
	± 0.08	± 0.36	± 0.17	± 0.06	± 0.11	± 0.23
$Var_{avg,inter}$ [mm]	0.41	0.47	0.37	0.37	0.37	0.60
$Var_{max,inter}$ [mm]	0.46	0.52	0.41	0.41	0.43	0.79
time [s]	216	126	134	205	143	416
	± 89	± 67	± 34	± 74	± 51	± 254
constraints set	47	32	40	82	47	52
	± 4	± 12	± 12	± 43	± 15	± 22

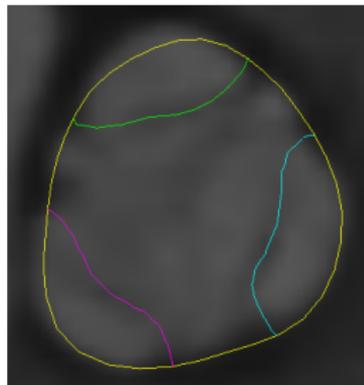
Editing of the aortic leaflets



Initialization

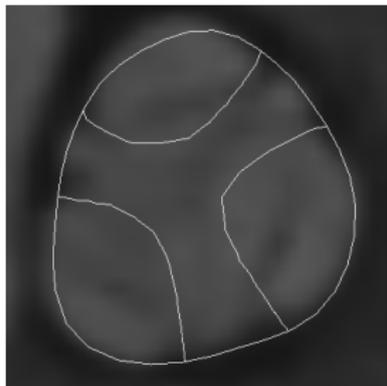


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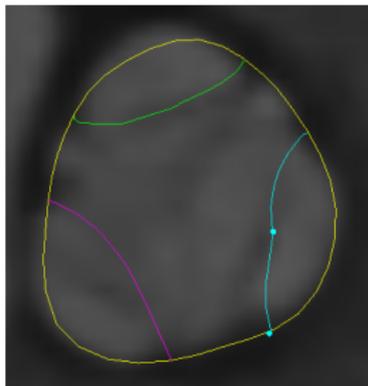


Local Editing

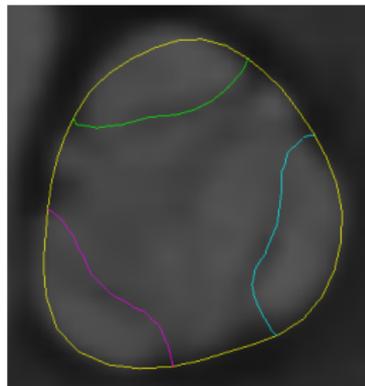
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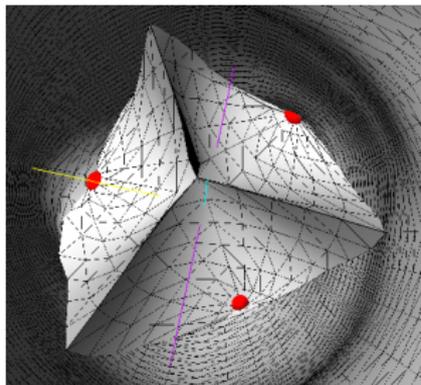
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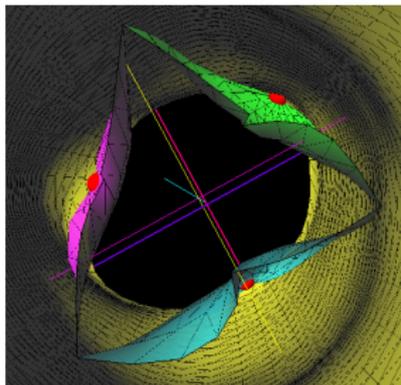
Local Editing

- valve closed after initial fully-automatic detection
- image data shows an open valve
- valve opening as editing step

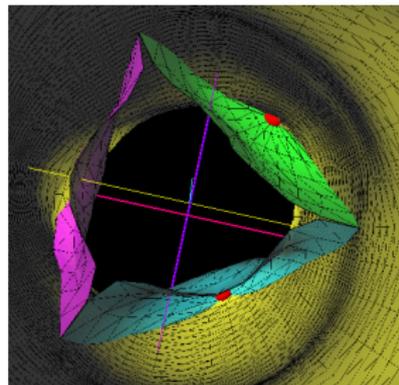
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Initialization

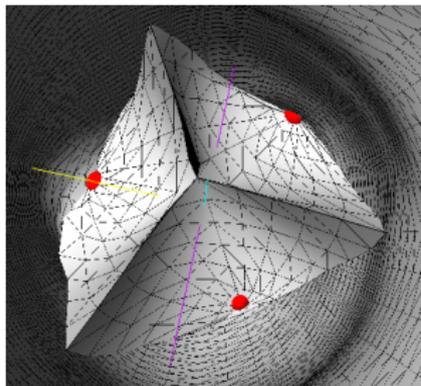


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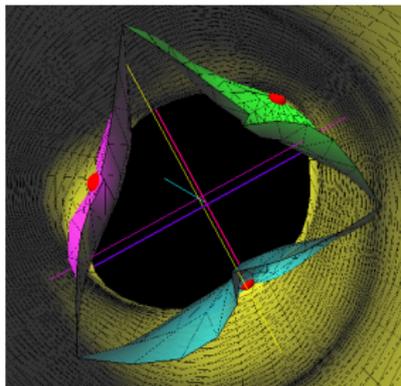


Local Editing

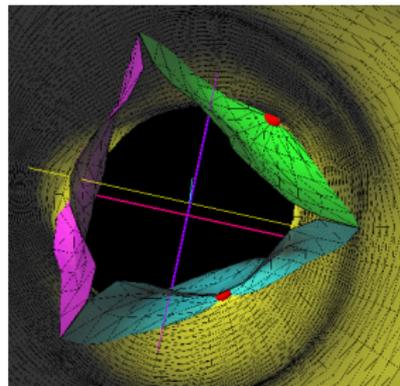
Editing of the aortic leaflets



Initialization



ARAP Editing



Local Editing

- acute angles at leaflet tip vertices in the middle are detail features
- detail features can not be easily eliminated with ARAP
- better results here with local editing

Outlook

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Evaluation for ...

- ... mitral valve editing
- ... editing of the right heart valves
- ... four-chamber segmentation editing
- ... other organs like e.g. the liver

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Snapping and shape validation based on other image features

- Canny edge detector
- features obtained by learning-based methods

Summarization

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Enhance efficiency and accuracy by involving image data ("edge snapping")

Sources

- Ionasec, R.I. ; Voigt, I. ; Georgescu, B. ; Yang Wang ; Houle, H. ; Vega-Higuera, F. ; Navab, N. ; Comaniciu, D.: *Patient-Specific Modeling and Quantification of the Aortic and Mitral Valves From 4-D Cardiac CT and TEE*.
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Thank you for your attention!